

Towards At-Home Applications of Pulse Wave Imaging (PWI): Investigating Optimal Sampling Parameters for Real-Time Pulse Wave Velocity (PWV) Estimation

Introduction

Pulse Wave Imaging (PWI)¹⁻⁷

- Quantification of central arterial mechanics can improve the characterization and monitoring of cardiovascular-related diseases including hypertension, diabetes, Alzheimer's, etc.⁸
- PWI is a **noninvasive**, **high-frame-rate**, **ultrasound imaging** method that tracks the pulse wave propagation
- PWI provides estimates of **central arterial properties** (carotid, aorta), including pulse wave velocity (PWV) at end-diastole (PWV_{ED}) and end-systole (PWV_{ES}), pulse pressure (PP), compliance, and homogeneity

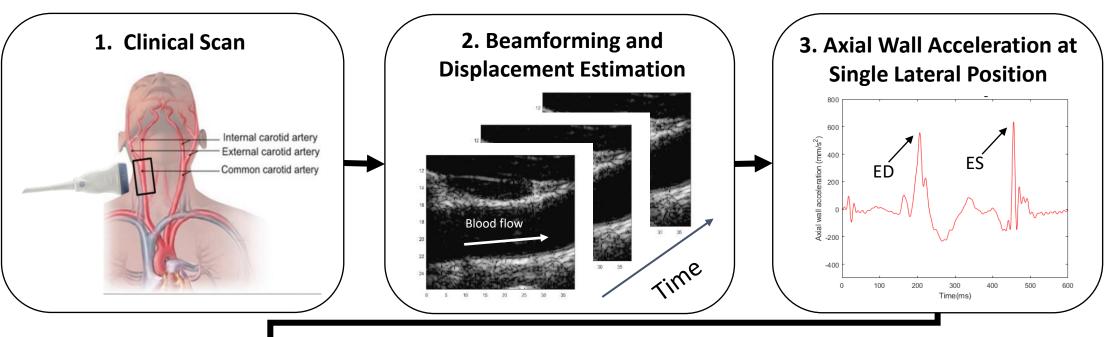
Translation of PWI to At-Home and Wearable Applications

- Advancements in piezoelectric micromachined ultrasound technology (**PMUT**) have enabled the development of **at-home** and **wearable** applications of PWI⁹⁻¹⁰
- Current PWI technique requires offline processing (~13-18 minutes) and GPU-based computing
 - Home-Use Requirements: Real-time PWV and PP estimation (within 1-2 minutes of the scan)



PWI Pipeline:

Figure 1. 3D-printed holder for PMUT array (left) compared to the conventional L7-4 linear transducer (right)



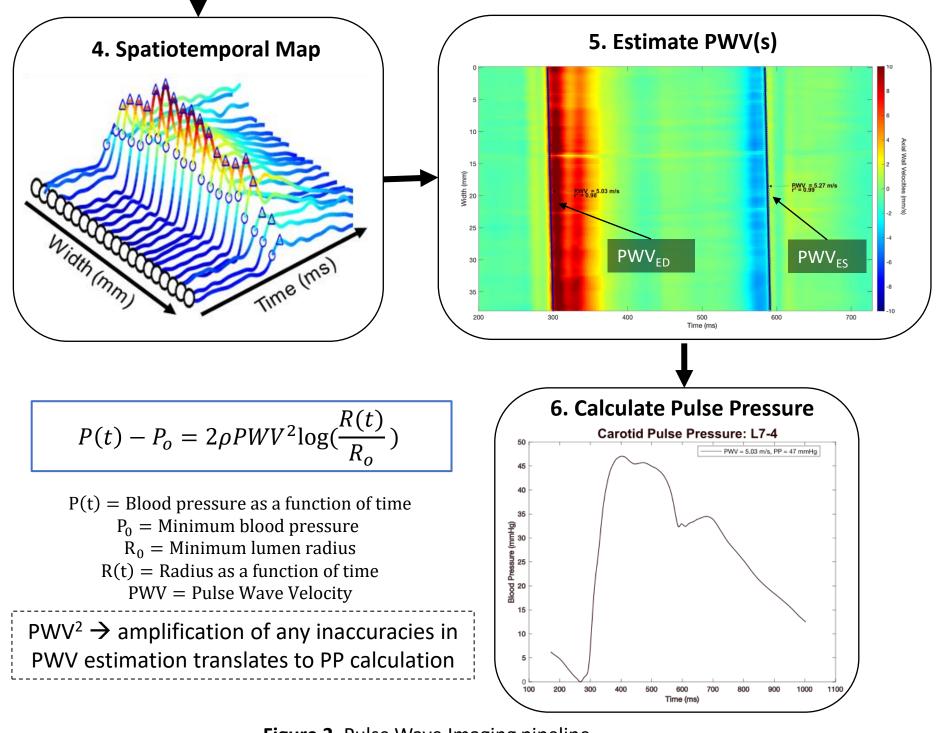


Figure 2. Pulse Wave Imaging pipeline

Objective: To guide the development of Real-Time PWI.

- Determine the minimum number of lateral positions necessary for accurate PWV estimation
- Compare sampling strategies between data collected from the PMUT array (future at-

home/wearable) and L7-4 transducer (conventional diagnostics transducer)

References

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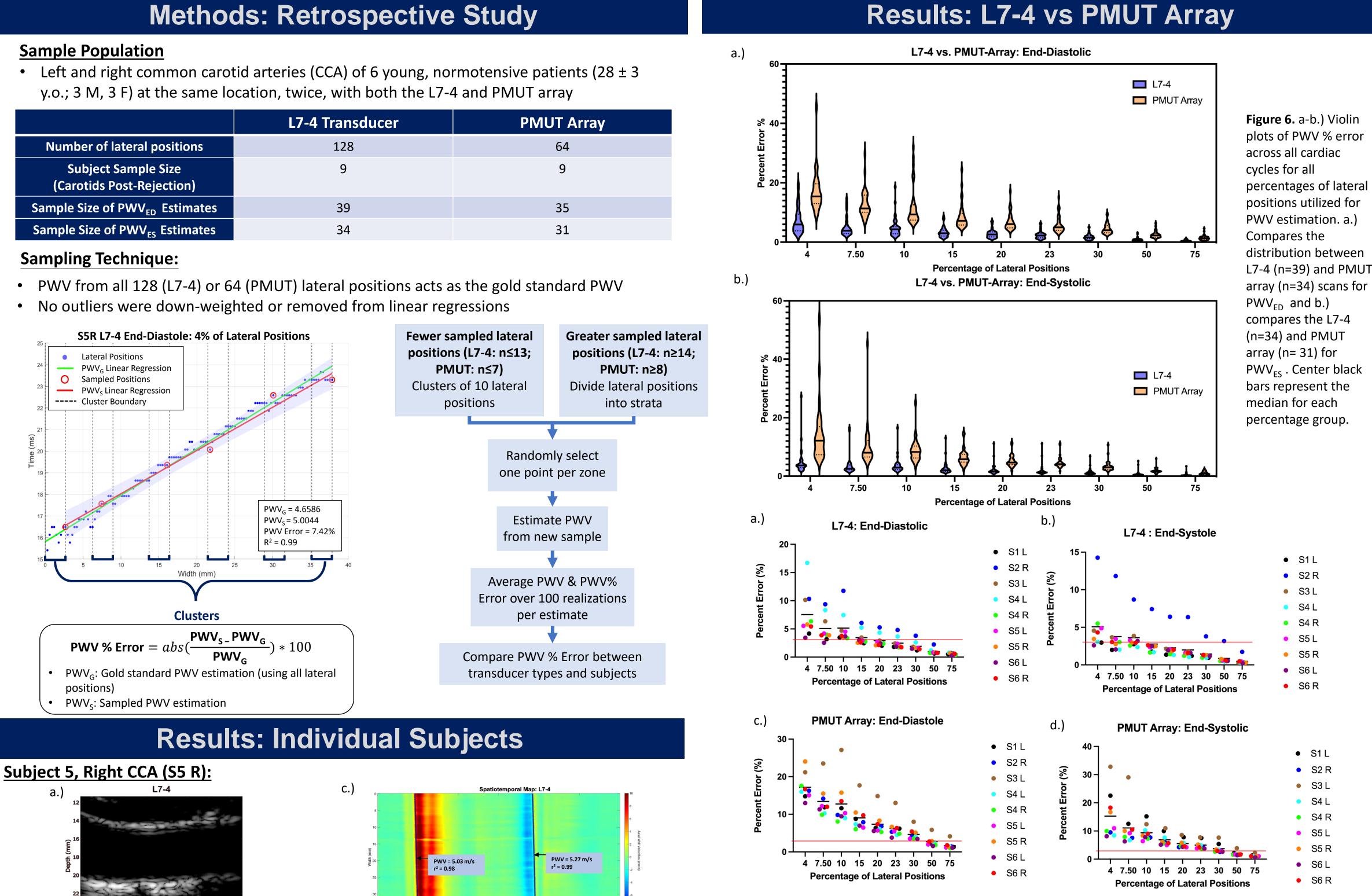
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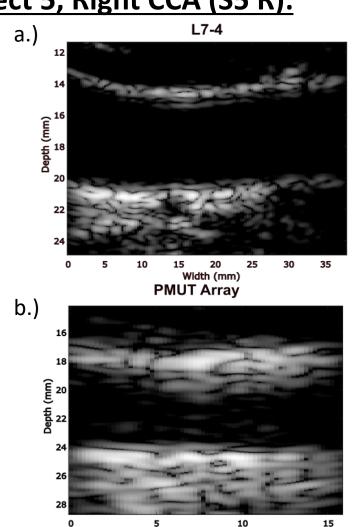
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y.o.; 3 M, 3 F) at the same location, twice, with both the L7-4 and PMUT array

	L7-4 Transducer	PMUT Array
Number of lateral positions	128	64
Subject Sample Size (Carotids Post-Rejection)	9	9
Sample Size of PWV _{ED} Estimates	39	35
Sample Size of PWV _{ES} Estimates	34	31

Sampling Technique:





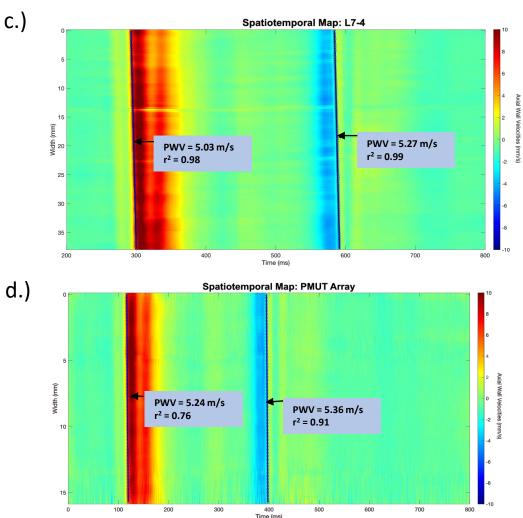


Figure 4. a-b.) B-modes of \$5 R's right CCA acquired from L7-4 transducer and PMUT Array, respectively. c-d.)Spatiotemporal maps and corresponding pulse wave velocity estimates for the data collected by the L7-4 (a) and PMUT array (c)



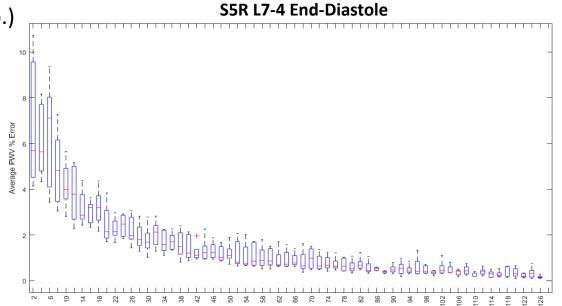


Figure 5. a.) Average estimated PWV_{FD} values from 2-128 lateral positions utilized for S5's right CCA using L7-4. Each colored line represents a different cardiac cycle and single PWV estimate; the black line represents the average of all cycles. b.) Box plots for the average PWV % error across all cardiac cycles for S5 R from utilizing 2-128 lateral positions.

Figure 7. a-d.) The PWV% error values for all cardiac cycles per carotid artery (n=9) were averaged and plotted from the L7-4 (a-b) and PMUT array (c-d). The black bars represent the mean PWV % error across all subjects for each percentage group of lateral positions utilized for PWV estimation. Red lines are located at 3% error.

Conclusions

Minimum Percentage of Lateral Positions for PWV Error < 3%	L7-4 Transducer	PMUT Array
PWV _{ED}	20-23% (26-30 positions)	47-63% (30-40 positions)
PWV _{ES}	15-23% (20-30 positions)	40-53% (26-34 positions)

PWV estimations using the PMUT array will give similar results to L7-4 when averaged over multiple cardiac cycles—however, real-time estimation will require a higher percentage of lateral positions for PWV estimation when using PMUT.

Future work:

Increase patient population and variability (larger age-range, include subjects with vascular disease, etc.), development of live quality standards to improve the selection of lateral positions in cluster-bands

Acknowledgements

This study was supported by the Amazon Summer Undergraduate Research Experience (SURE) Fellowship. Data utilized in this study was collected with financial support from the National Institutes of Health (NIH RO1HL167085-01A1) and the TDK Corporation.

